



Maintenance and Neuronal Cell Differentiation of Neural Stem Cells C17.2 Correlated to Medium Availability Sets Design Criteria in Microfluidic Systems

Bu Wang¹, Sabrina Jedlicka^{1,2}, Xuanhong Cheng^{1,2*}

1 Department of Materials Science and Engineering, Lehigh University, Bethlehem, Pennsylvania, United States of America, **2** BioEngineering Program, Lehigh University, Bethlehem, Pennsylvania, United States of America

Abstract

Background: Neural stem cells (NSCs) play an important role in developing potential cell-based therapeutics for neurodegenerative disease. Microfluidics has proven a powerful tool in mechanistic studies of NSC differentiation. However, NSCs are prone to differentiate when the nutrients are limited, which occurs unfavorable by fast medium consumption in miniaturized culture environment. For mechanistic studies of NSCs in microfluidics, it is vital that neuronal cell differentiation is triggered by controlled factors only. Thus, we studied the correlation between available cell medium and spontaneous neuronal cell differentiation of C17.2 NSCs in standard culture medium, and proposed the necessary microfluidic design criteria to prevent undesirable cell phenotype changes.

Methodology/Principal Findings: A series of microchannels with specific geometric parameters were designed to provide different amount of medium to the cells over time. A medium factor (*MF*, defined as the volume of stem cell culture medium divided by total number of cells at seeding and number of hours between medium replacement) successfully correlated the amount of medium available to each cell averaged over time to neuronal cell differentiation. *MF* smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hour}$ produced significant neuronal cell differentiation marked by cell morphological change and significantly more cells with positive β -tubulin-III and MAP2 staining than the control. When *MF* was equal or greater than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hour}$, minimal spontaneous neuronal cell differentiation happened relative to the control. *MF* had minimal relation with the average neurite length.

Significance: *MF*s can be controlled easily to maintain the stem cell status of C17.2 NSCs or to induce spontaneous neuronal cell differentiation in standard stem cell culture medium. This finding is useful in designing microfluidic culture platforms for controllable NSC maintenance and differentiation. This study also offers insight about consumption rate of serum molecules involved in maintaining the stemness of NSCs.

Citation: Wang B, Jedlicka S, Cheng X (2014) Maintenance and Neuronal Cell Differentiation of Neural Stem Cells C17.2 Correlated to Medium Availability Sets Design Criteria in Microfluidic Systems. PLoS ONE 9(10): e109815. doi:10.1371/journal.pone.0109815

Editor: Wenhui Hu, Temple University School of Medicine, United States of America

Received: February 11, 2014; **Accepted:** September 12, 2014; **Published:** October 13, 2014

Copyright: © 2014 Wang et al. This is an open-access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

Funding: Funding for the research is provided by National Science Foundation (<http://www.nsf.gov/>) under Grant No. 1014957. The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the manuscript.

Competing Interests: The authors have declared that no competing interests exist.

* Email: xuc207@lehigh.edu

Introduction

Neural stem cells (NSCs) have recently attracted significant interest for their promise in treating neurodegenerative disorders, such as Alzheimer's disease, ischemia and Parkinson's disease. [1–12] Despite progress in neuronal cell differentiation and transplantation of NSCs, future success will require further understanding of the neuronal cell differentiation mechanisms. [2,4,5,7,9–11,13–20] Microfluidics has recently been shown to be a powerful tool in stem cell research, due to the advantage of precise control of individual environmental cues, single cell analysis, real-time measurement and easy integration with electrical stimulation. [21–46].

Concentration gradients of cytokine or growth hormone have been created in microfluidic devices to quantitatively study chemical and biological cues that initiate or facilitate neuronal cell differentiation. [22,47–50] Microfluidics have also been used

to introduce mechanical or topographical stimulation for the analysis of non-chemical cues on neuronal cell differentiation. [51,52] The use of microfluidics in NSC research, however, presents an issue with regard to dynamic nutrient concentration. As the culture volume is miniaturized, nutrient consumption from cell metabolism is much more pronounced than conventional bulk culture, while it is well established that NSCs are extremely sensitive to serum depletion. *In vivo* neuronal cell differentiation of NSCs occurs when there is a shortage of blood and oxygen supply, as studied in disease models like ischemia. [4,15,16,53–58] For *in vitro* cultures, serum withdrawal is often used to induce neuronal differentiation of NSC. [59–61] Based on the available knowledge up to date, we hypothesize that NSCs could undergo neuronal cell differentiation even in the regular NSC culture media if the volume of media available is limited, which after cell metabolism quickly becomes nutrient depleted. While it is desirable to induce differentiation through controlled biological,

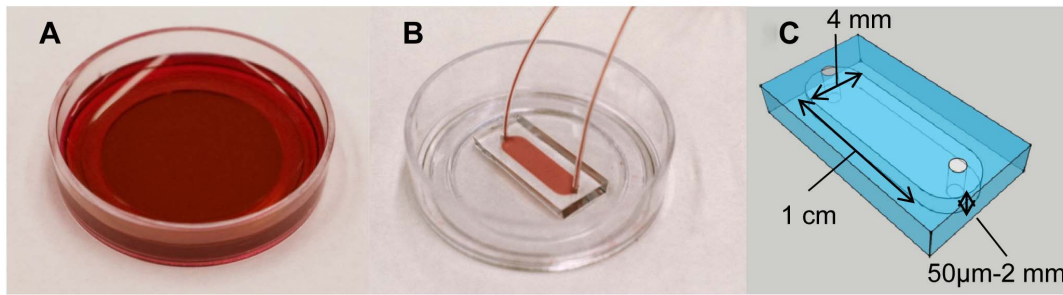


Figure 1. A control and PDMS bonded FluoroDish for cell culture. (A) A standard bulk culture on FluoroDish was used as the control. (B–C) PDMS microchannels with a footprint of 1 cm×4 mm (L×W) and various heights (50 μm, 250 μm, 500 μm, 1 mm and 2 mm) were permanently bonded to FluoroDish to control the amount of medium available to cells. The microchannels were autoclaved prior to bonding and cell culture. doi:10.1371/journal.pone.0109815.g001

chemical and physical cues, spontaneous differentiation needs to be characterized to guide microfluidic design and avoid its interference with mechanistic studies.

Here, we used microfluidic devices to control the amount of culture medium available and characterized the phenotype of C17.2 NSCs over three weeks in standard culture medium. C17.2 is an immortalized mouse neural progenitor cell line established by retroviral-mediated transduction of the avian *myc* oncogene into mitotic progenitor cells of neonatal mouse cerebellum, and an important model system in studies of neural regeneration. [9,11,12,59–67] C17.2 NSCs have shown the ability to successfully integrate into the central nervous system of animals used as disease models for Parkinson's, stroke and Alzheimer's. [9–12] Both *in vivo* and *in vitro* studies also demonstrate that C17.2 NSCs undergo neuronal cell differentiation under nutrient depletion, [11,12,59–61,64] which makes them an appropriate cellular model for this work. A medium factor (*MF*) was used as a quantitative measure of available medium to each cell per unit time. The *MF* was defined as the volume of culture medium normalized to the total number of cells at seeding and the feeding period. It was controlled using microchannels of various heights, since it is otherwise difficult to reduce the height of culture media to below one millimeter in conventional bulk culture, considering the meniscus. Another strategy to control *MF* was to vary the feeding frequency, with higher frequency making more fresh medium available to each cell over time. Cell morphology and quantified immunocytochemistry results were examined to verify the correlation between the resulting differentiated cell population and the *MF*. Critical thresholds of *MF* to maintain the stem cell characteristics were identified. The range of consumption rate of serum molecules involved in the process is also discussed in the paper.

Materials and Methods

Cell culture

Immortalized murine neural progenitor cells C17.2 (established cell line [9,11,12,59–67] as a generous gift to the Jedlicka Lab from Dr. Evan Snyder, of the Sanford-Burnham Medical Research Institute) were grown on 100 mm polystyrene tissue culture dishes (BioLite, Fisher Scientific) at 37°C in 5% CO₂ in air. The culture medium consisted of high glucose Dulbecco's modified Eagle medium (DMEM) (HyClone, Fisher Scientific) supplemented with 10% fetal bovine serum (HyClone, Fisher Scientific), 5% horse serum (TCS Biosciences) and 2 mM L-glutamine (MP Biomedicals).

Microfluidic device fabrication

Polydimethylsiloxane (PDMS) microchannels were prepared following the standard soft lithography protocol. Two types of molds were used in this study: SU8 was patterned on silicon wafers for devices with 50 μm and 250 μm heights; micromachined steel molds were used for devices with 500 μm, 1 mm and 2 mm heights. All devices had the same footprint of 1 cm×4 mm (L×W). A 10:1 mixture of silicone elastomer base and silicone elastomer curing agent (Sylgard 184 silicone elastomer kit, Dow Corning Corporation) was poured onto the molds, degassed, cured at 65–75°C and the microdevices were cut out. Fluid inlets and outlets were drilled using a syringe needle. Microchannels were then autoclaved at 121°C for 1 hour. Afterwards, glass bottomed petri dishes (FluoroDish, World Precision Instruments) and the PDMS microchannels were activated by oxygen plasma, carefully aligned and heated for 5–10 minutes at 65–75°C to produce permanent bonding. The control (a standard microwell culture) and one packaged microfluidic device are shown in Figure 1.

Table 1. The microchannel geometries and feeding conditions used in this study.

Microchannel height (μm)	Flow rate for cell feeding (μL/hr)	Vol. of medium (μL)	Feeding interval (hour)			
50	250	5	12	24	48	–
250	6,250	25	12	24	48	–
500	25,000	50	12	24	48	–
1000	100,000	100	12	24	48	–
2000	400,000	200	–	24	48	96

doi:10.1371/journal.pone.0109815.t001

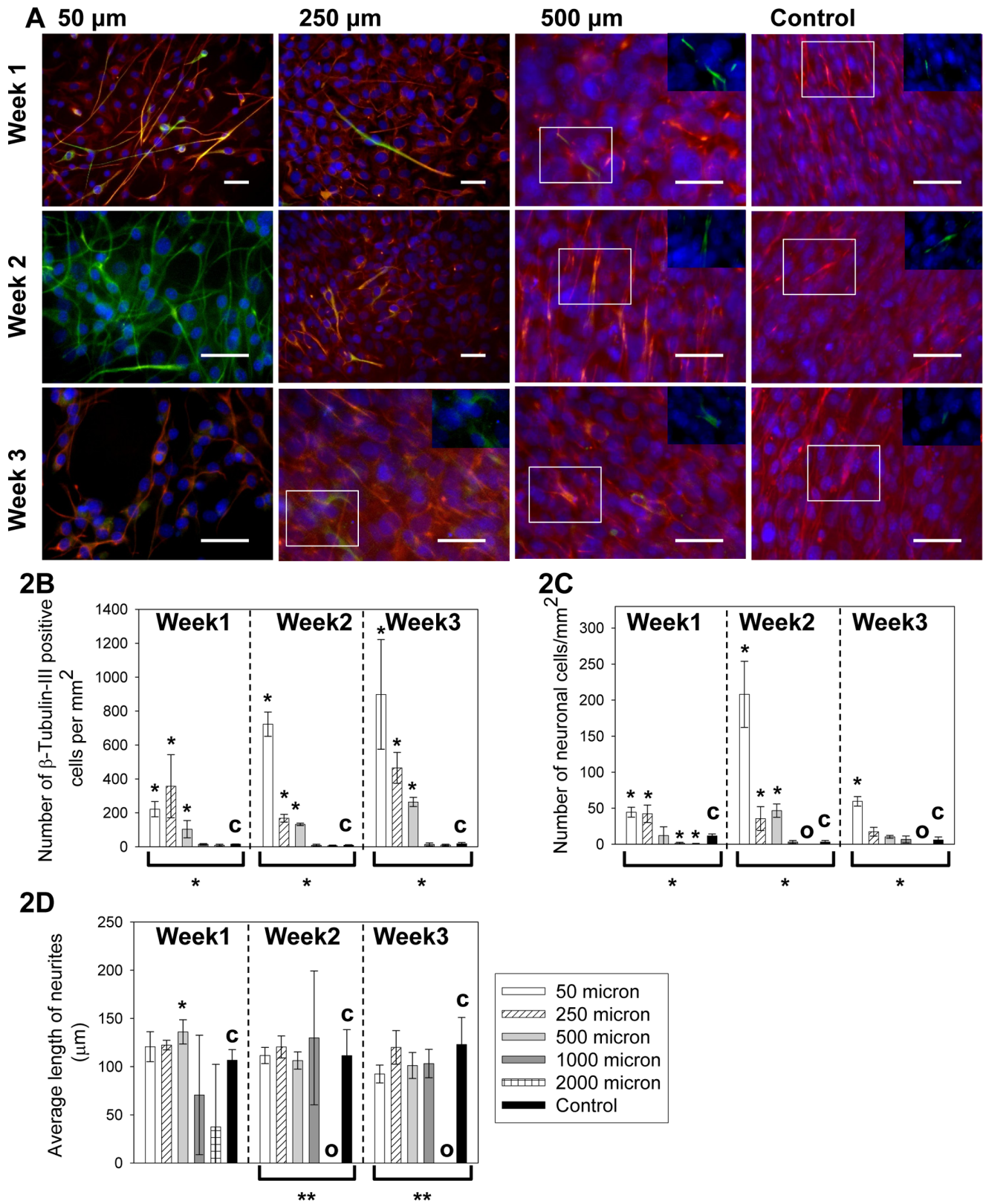


Figure 2. Neuronal cell differentiation of C17.2 cells cultured in microchannels with different heights of 50–2000 μm under a 48 hr feeding interval. (A) The cell morphological change over 3 weeks. Images from the 1000 and 2000 micron samples were not shown since they had similar morphology and staining results as the control for all three weeks. Red: Nestin. Green: β -tubulin-III. Blue: cell nuclei. In some samples, the β -tubulin-III staining was shadowed by the Nestin staining after triple overlay, due to the small number of spontaneously differentiated cells in these samples. In these samples, overlays of the β -tubulin-III and nuclei staining were shown in the inset from the boxed areas. Scale bar = 50 μm . The insets were at the same scale as the main images. (B) The β -tubulin-III positive cell counts per mm^2 over time. (C) The neuronal cell counts per mm^2 over time.

over time. (D) The average neurite length measurement over time. Bars with “O” in Figure 2C and Figure 2D indicated that no cell was identified as a neuronal cell. In Figures 2B–2D, the control (with “c”) was C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. Data were shown as mean \pm standard deviation. The * above the bars indicated a statistical difference between the sample and the control by two-tailed Student’s *t* test ($p < 0.05$). The */** below the bars indicated a statistical difference in the group by the one-way ANOVA test ($p < 0.05$). The ** in Figure 2D indicated a significant difference due exclusively to the samples with no neurite outgrowth. $N \geq 15$.
doi:10.1371/journal.pone.0109815.g002

Cell maintenance and differentiation in microchannels

Trypsinized and suspended C17.2 NSCs were injected into microchannels of different heights: 50 μm , 250 μm , 500 μm , 1 mm and 2 mm. The suspension concentration was adjusted so the surface density was comparable in all devices and was $\sim 25,000$ cells/ cm^2 after initial cell adhesion. After allowing the cells to adhere for 3 hours, the cells were fed periodically every 12, 24, 48 or 96 hours using a syringe pump. Flow rates were used to generate a comparable wall shear stress of 0.004 Pa in all devices. A total of 2.5 times the device volume was injected at every time interval to ensure complete medium replacement. Table 1 summarizes the conditions used. The flow pattern and feeding interval combination was determined by preliminary experiments (Figure S1, Figure S2 and Figure S3). As a control, C17.2 cells were seeded at the same surface density into a FluoroDish without any microchannel. The medium in the control was withdrawn completely and replaced every 48 hours (standard subculture feeding frequency). All devices were kept under humidified environment at 37°C in 5% CO₂ in air. Three samples in each condition were immunostained after 1 week, 2 weeks and 3 weeks of culture to monitor the cell phenotype over time. At least five images were captured at random locations from each sample, thus a total of 15 images or more were analyzed under each condition.

Immunostaining

Cells were fixed in 3.7% paraformaldehyde (Sigma-Aldrich) for 15 min, permeabilized with 0.1% Triton X-100 (Fisher Scientific) in phosphate buffered saline (PBS, Fisher) for 15 min, and blocked by 1% bovine serum albumin (BSA, Sigma-Aldrich) in 0.01% Triton X-100 for 15 min at room temperature. Both primary and secondary antibodies were diluted in 0.1% BSA and 0.001% Triton X-100 solution and then incubated with cells overnight for 8–10 hrs at 4°C. Primary antibodies used were Nestin (clone Rat-401, Fisher Scientific), anti- β -tubulin-III (AlexaFluor488, clone TUJ1, BD Biosciences) and anti-MAP2 antibody (AlexaFluor488, clone AP20, Chemicon). The secondary antibody for Nestin was AlexaFluor546 anti-mouse IgG₁ (Invitrogen). Finally cell nuclei were stained with 0.002 mg/ml Hoechst No. 33258 (Invitrogen) for 5 min. After rinse, 5 images were captured from each sample using phase-contrast and fluorescence microscopy (Eclipse TE2000U, Nikon). The surface area in each image was 0.15 mm^2 . The average number of β -tubulin-III positive cells per mm^2 was calculated to characterize the onset of neuronal cell differentiation. MAP2 staining was carried out in selected sets of samples: 50 μm tall microchannel samples under a 48 hr feeding interval, 2 mm tall microchannel samples under a 48 hr feeding interval and fluorodish samples under a 48 hr feeding interval, to confirm the results from β -tubulin-III staining.

Neurite measurement

The lengths of neurites were measured using immunostained images. Cells with positive staining by β -tubulin-III and neurite outgrowth greater than two times the size of soma were considered as neuronal cells. Neurite outgrowth from each neuronal cell was measured by the NeuronJ plugin in ImageJ (National Institutes of Health). The average number of neuronal cells per mm^2 was used

to characterize neuronal cell differentiation. The average neurite length (total neurite length divided by the number of neurites in an image) was also calculated.

Medium factor (MF)

The MF was introduced to quantify the amount of medium available to cells over the feeding period. It was calculated by the following equation:

$$MF = \frac{V}{P \times t}$$

Where V is the volume of culture medium, P is the total number of cells at seeding, t is the time interval between two feeding events.

Data analysis

All data sets in graphs are presented as average \pm standard deviation from repeats in at least three independent devices. When comparing multiple samples in a group, one-way ANOVA test was used with a p -value of 0.05. When comparing test samples to the control, two-tailed Student’s *t* test was used with a p -value of 0.05.

Results and Discussion

C17.2 differentiation in microchannels with different heights but fixed feeding frequency

First, we examined C17.2 NSCs cultured in microchannels with different heights under fixed feeding frequency. In this case, the MF scales linearly with the microchannel height. As a control, cells were seeded at the same surface density in FluoroDish without microchannels (with “c” in all graphs). The average medium height in the open culture is ~ 2 mm, calculated by the volume of medium divided by the surface area of the dish bottom, and the cells were fed every 48 hours as in standard subculture protocols.

The progression of cell morphology over time is shown in Figure 2A and the quantified immunocytochemistry results are shown in Figure 2B–D. As shown in Figure 2A, groups with lower MF values (50 μm , 250 μm and 500 μm microchannels) began to have morphological change consistent with neuronal cell differentiation after 1 week. This trend became dominant after 2 weeks with the 50 μm microchannel yielding almost a pure population of cells with neurite outgrowth and positive β -tubulin-III staining. On the other hand, Nestin staining (red) weakened on the elongated cells, and became nearly undetectable in the 50 μm group in week 2, also suggesting neuronal cell differentiation. When the images were analyzed quantitatively, the cell populations in 50 μm , 250 μm and 500 μm microchannels were found to show significantly higher number of β -tubulin-III positive cells compared to the control (with * above the bars, p values range from 0.00001 to 0.04) over the entire experimental course of 3 weeks (Figure 2B). The β -tubulin-III positive cell number continued to grow over time, demonstrating an overall tendency towards the neuronal cell differentiation fate. However, neuronal cells (defined here as β -tubulin-III positive cells with neurite length longer than two times that of soma) peaked around 2 weeks and degenerated afterwards (Figure 2A and Figure 2C), as seen by

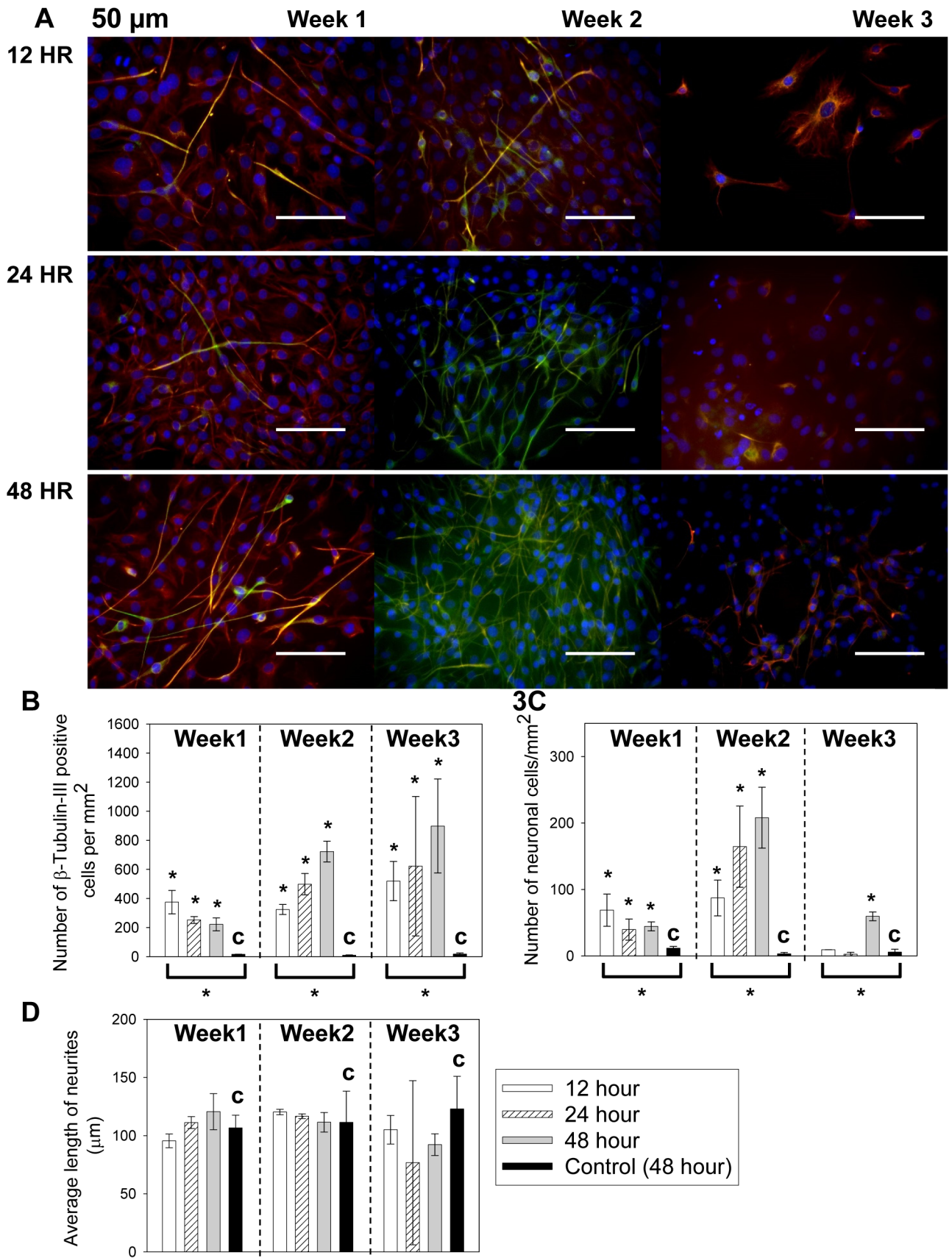


Figure 3. Neuronal cell differentiation of C17.2 cells cultured in 50 μm microchannels with 12, 24 and 48 hour feeding intervals. (A) The cell morphological change over 3 weeks. All groups showed biomarker staining and morphological change consistent with neuronal cell

differentiation. Red: Nestin. Green: β -tubulin-III. Blue: cell nuclei. Scale bar = 100 μm . (B) The β -tubulin-III positive cell counts per mm^2 over time. (C) The neuronal cell counts per mm^2 over time. (D) The average neurite length measurement over time. In Figures 3B–3D, the control (with “c”) was C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. Data were shown as mean \pm standard deviation. The * above the bars indicated a statistical difference between the sample and the control by two-tailed Student’s *t* test ($p < 0.05$). The * below the bars indicated a statistical difference in the group by one way ANOVA ($p < 0.05$). $N \geq 15$.

doi:10.1371/journal.pone.0109815.g003

reduction of the neuronal density and weaker β -tubulin-III staining at week 3. The 50 μm microchannel showed significantly higher number of neuronal cells compared to the controls (with * above, p values range from 0.0003 to 0.0015) at all time points. The 250 μm microchannel showed significantly higher number of neuronal cells compared to the controls (with * above, p values are 0.013 and 0.028 respectively) in the first 2 weeks. The 500 μm microchannel showed significantly more neuronal cells than the control only in week 2 (with * above, $p = 0.001$), but not in week 1 or 3. The 1000 μm and 2000 μm samples, on the other hand, showed comparable or lower level of neuronal cell differentiation compared to the control, as demonstrated by lack of morphological change (images similar to those of the control, not shown) as well as the low number of β -tubulin-III positive cells (Figure 2B) and a baseline presence of neuronal cells (Figure 2C). For the 500 μm microchannel, the average neurite length was slightly higher than the control after 1 week of culture (with * above, $p = 0.04$). The average neurite length (Figure 2D) was the same for the rest of the test conditions and time points (p values range from 0.09 to 1), except for those lacking observable neurites (with “O” in Figure 2C and Figure 2D). The low level of neuronal differentiation limits the data points collected from the tall channels (1000 and 2000 μm), resulting in large standard deviation in Figure 2D. Samples from different channel heights but the same weeks were further analyzed using ANOVA. Groups with statistical difference among the samples ($p < 0.05$) were marked by brackets and * underneath. For the density of β -tubulin-III positive cells and neurons, the various device heights led to statistically different results at the same time point. For the neurite length comparison, the device height did not create significant difference at week 1. The significant difference of neurite length observed at week 2 and week 3 (with ** underneath, $p < 0.05$) was due exclusively to samples with zero neurite outgrowth in the groups. Thus, the neurite length was comparable among all samples with detectable neurite outgrowth at the same week.

C17.2 differentiation in microchannels with fixed geometry but different feeding frequencies

Next, cell behavior was compared for cultures fed under different frequencies but in microchannels with fixed heights. In this case, the *MF* scales linearly with the reverse of the time interval.

The morphological change of cells in 50 μm microchannel over time is shown in Figure 3A and the quantified immunocytochemistry results are shown in Figure 3B–D. In all the groups, cells began to develop smaller cell bodies and neurite outgrowth after 1 week (Figure 3A). After 2 weeks more cells showed neural morphology and positive β -tubulin-III staining. At the same time, the β -tubulin-III staining became stronger as Nestin staining weakened. After 3 weeks of culture, the cells with long neurites started to deteriorate. Instead, another population with flattened cell body and relatively short and unbranched processes began to dominate, which co-expressed both Nestin and β -tubulin-III. As shown in Figure 3B, the cell populations in 12 hr, 24 hr and 48 hr groups all showed significantly higher number of β -tubulin-III

positive cells than the control in all 3 weeks (with * above, p values range from 0.00006 to 0.009). The β -tubulin-III positive cell number increased constantly over time, indicating a steady population growth in the overall neuronal cell differentiation path. The large error bars for samples in week 3 are caused by non-uniformly distributed cell population mixture associated with neuronal degeneration. The numbers of neuronal cells are shown in Figure 3C. The initial growth, peak growth and deterioration of neuronal cells were observed in all groups. At initiation and peak stages, all groups showed significantly higher number of neuronal cells compared to the control (with * above, p values range from 0.002 to 0.04). At week 3, the difference in neuronal cell number between the microfluidic groups and the control diminished, except for the group with lowest *MF* (with * above, 48 hours, $p = 0.0003$). The average neurite length was comparable for all groups (p values range from 0.15 to 1) as shown in Figure 3D. The large standard deviation of neurite length at week 3 is a result of neuronal degeneration, leaving behind a mixed population of cells with broad distribution of neurite length. The ANOVA test of different feeding conditions at each time point indicated that the feeding intervals significantly impacted the density of β -tubulin-III positive cells and neurons in the 50 μm channels (brackets and * underneath the groups, $p < 0.05$), but not the neurite length ($p > 0.05$).

The morphology change of cells over time in 250 μm microchannel is shown in Figure 4A and the quantified immunocytochemistry results are shown in Figure 4B–D. The cell populations in 24 hr and 48 hr groups showed neurite outgrowth (Figure 4A) and significantly higher number (Figure 4B) of β -tubulin-III positive cells than the control at all time points (with * above the bars, p values range from 0.0003 to 0.03). However, the 12 hr group had minimal morphological change (Figure 4A) over 3 weeks. The numbers of β -tubulin-III positive cells in the 12 hr group were comparable to the control at all stages (p values range from 0.07 to 1). The numbers of neuronal cells are shown in Figure 4C. The initial growth, peak growth and deterioration of neuronal cells were observed in 24 hr and 48 hr groups. At the peak stage, groups with lower *MF* values, i.e. with 24 hr and 48 hr feeding intervals, showed significantly higher number of neuronal cells than the control ($p = 0.00004$ and 0.028 respectively). The 12 hr group with higher *MF* started with significantly lower number of neuronal cells comparing to the control (with * above, $p = 0.03$), but the difference became insignificant later ($p = 0.4$ at 2 weeks and $p = 0.3$ at 3 weeks). The average neurite length was comparable to the control for all the samples (p values range from 0.09 to 0.9) as shown in Figure 4D. The ANOVA test for the 250 μm samples at each week also indicated that the density of β -tubulin-III positive cells and neurons changed significantly with the feeding intervals (brackets and * underneath the groups, $p < 0.05$), but not the neurite length.

To ensure that the increase in neuronal cell differentiation observed in microchannels were due to the nutrient concentration but not PDMS or feeding under a flow condition, cell population in 2000 μm microchannels was compared to that in bulk culture (Figure 5), as the *MF* factors were similar in these cases. Little morphological and biomarker change was observed over time in

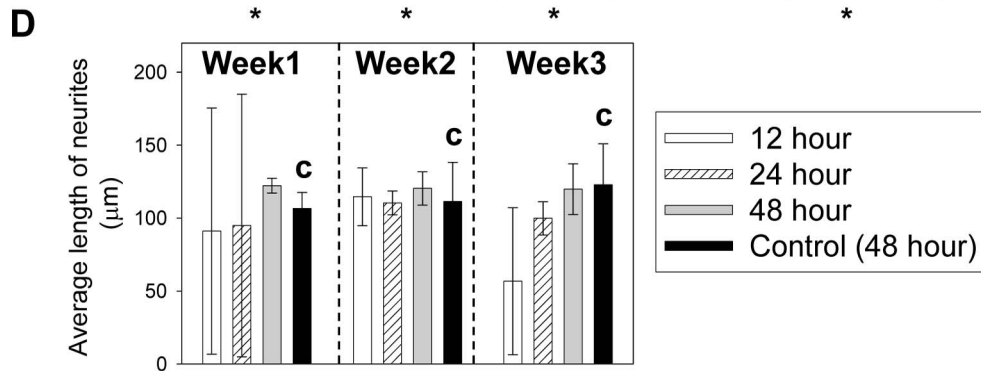
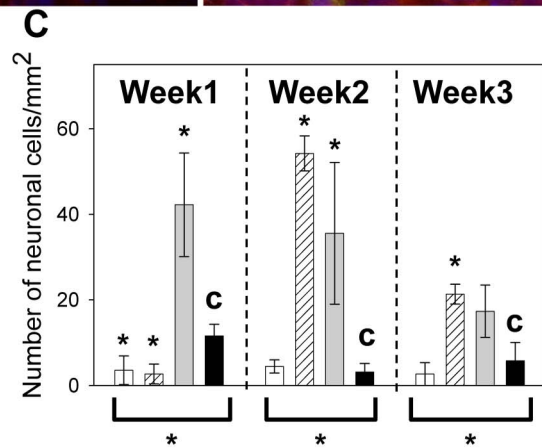
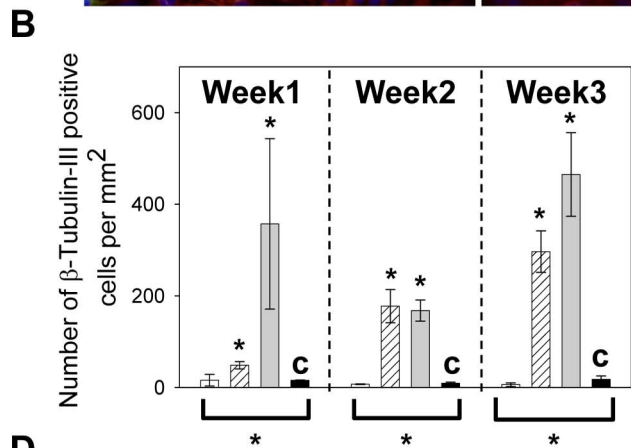
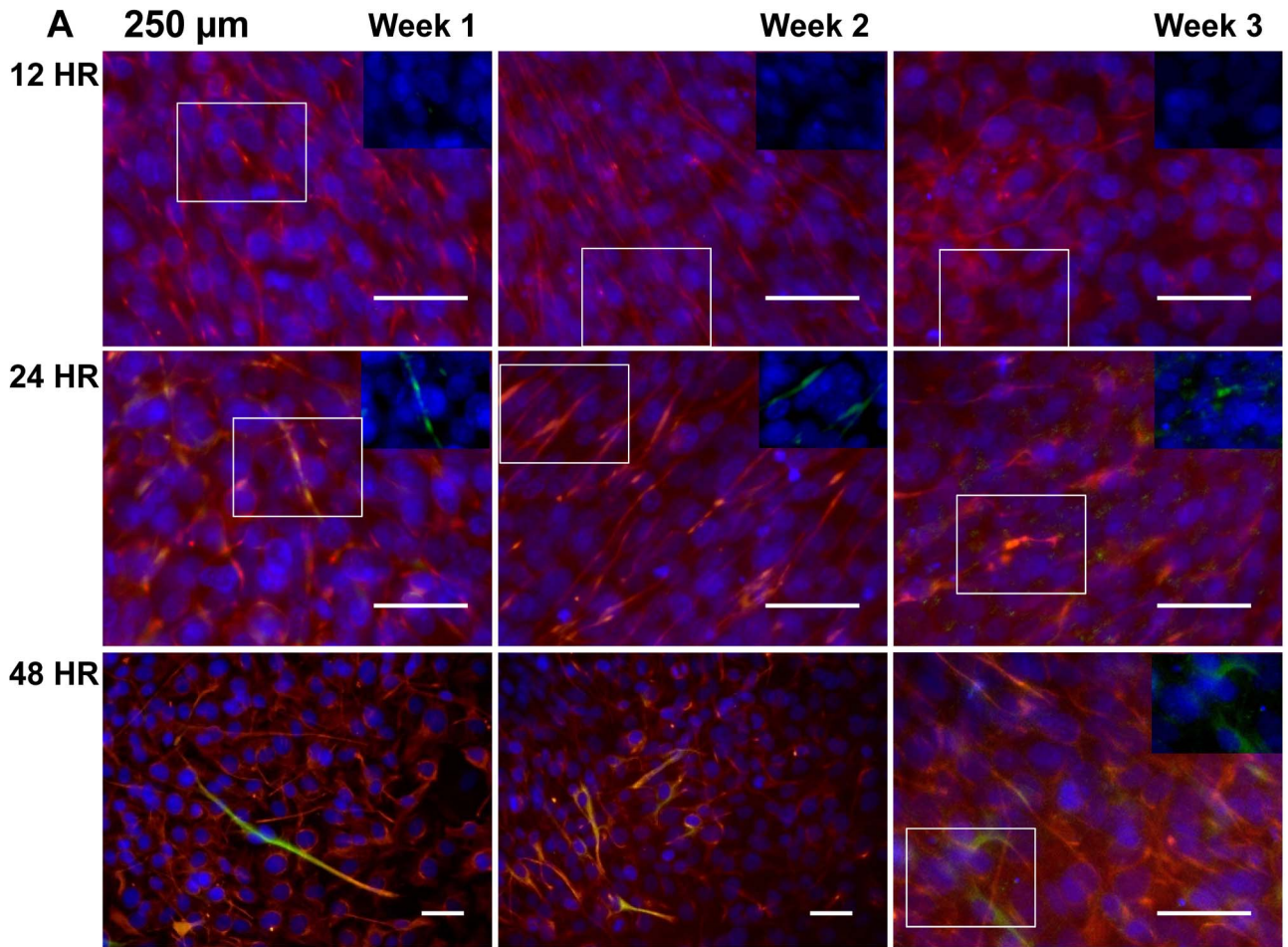


Figure 4. Neuronal cell differentiation of C17.2 cells cultured in 250 μm microchannels with 12, 24 and 48 hour feeding intervals.

(A) The cell morphological change over 3 weeks. To better demonstrate the positive β-tubulin-III staining in the 24 hour and 48 hour samples, overlays of the β-tubulin-III and nuclei staining were shown in the inset from the boxed areas. In comparison, insets of β-tubulin-III and nuclei staining were also shown for the 12 hour samples, but β-tubulin-III staining was not visible. Red: Nestin. Green: β-tubulin-III. Blue: cell nuclei. Scale bar = 50 μm. The insets were from the boxed region and were at the same scale as the main images. (B) The β-tubulin-III positive cell counts per mm² over time. (C) The neuronal cell counts per mm² over time. (D) The average neurite length per mm² over time. In Figures 4B-4D, the control (with “c”) was C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. Data were shown as mean ± standard deviation. The * above the bars indicated a statistical difference between the sample and the control by two-tailed Student’s t test ($p < 0.05$). The * below the bars indicated a statistical difference in the group by one way ANOVA ($p < 0.05$). $N \geq 15$.

doi:10.1371/journal.pone.0109815.g004

all samples (images not shown), demonstrating minimal neuronal cell differentiation. When the results were quantitatively analyzed, the cell population with the 24 hr feeding intervals showed lower number of β-tubulin-III positive cells compared to the control (Figure 5A) at 1 week (with * above, $p = 0.00004$). This is possibly due to more thorough medium replacement in microfluidics as compared to traditional pipetting in petri dishes: the channel is flushed with fresh medium 2.5 times the channel volume at every cell feeding, while in traditional petri dish culture, the old medium is suctioned up and replaced with equal volume of fresh medium once. The rest of the microfluidic samples shared comparable number of β-tubulin-III positive cells to the control (p values range from 0.08 to 0.9). As shown in Figure 5B, all samples had lower number of neuronal cells compared to the control in the first week

(p values range from 0.02 to 0.04), but the difference diminished later. From Figure 5C, it was observed that the average neurite length of most samples were similar to the control except for those without noticeable neurite outgrowth (with “O” in Figure 5B and Figure 5C). The ANOVA tests for samples from the same time points demonstrated comparable density of β-tubulin-III cells and neurite length in the 2000 μm channels. The density of neuronal cells were significantly different under the various feeding intervals (brackets and * underneath the groups, $p < 0.05$), but the difference was due to a reduced neuronal density than the control. The neurite length was comparable. The ** in Figure 5C and 5D indicate difference due exclusively to the samples with zero positive cells. These results support that the enhanced neuronal cell differentiation associated with low channel

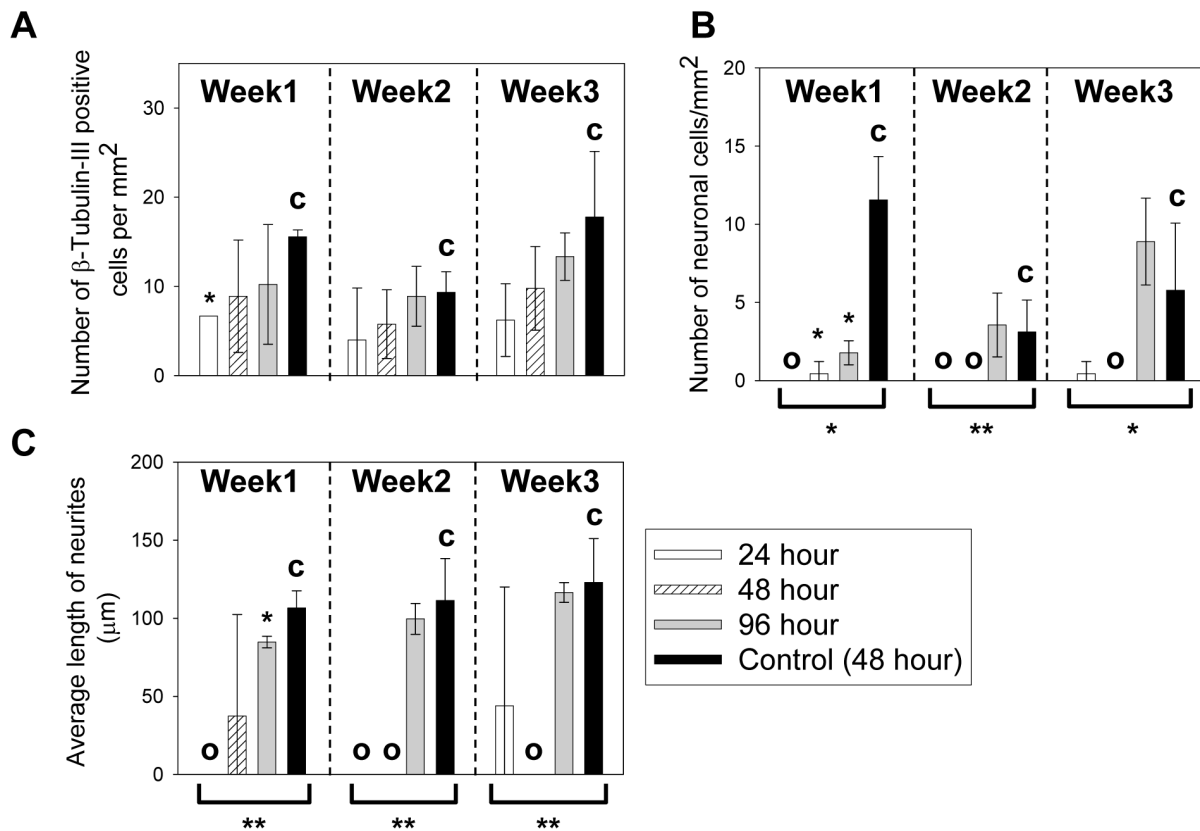


Figure 5. Behavior of C17.2 cells cultured in 2000 μm microchannels with 24, 48 and 96 hour feeding intervals. (A) The β-tubulin-III positive cell counts per mm² over time. (B) The neuronal cell counts per mm² over time. (C) The average neurite length per mm² over time. Groups lacking neuronal cells were labeled with “O” in Figure 5B and Figure 5C. The control (with “c”) was C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. The * above the bars indicated a statistical difference between the sample and the control by two-tailed Student’s t test ($p < 0.05$). The * below the bars indicated a statistical difference in the group by one way ANOVA ($p < 0.05$). The ** in Figure 5C indicates a significant difference due exclusively to the samples with no neurite outgrowth. $N \geq 15$.

doi:10.1371/journal.pone.0109815.g005

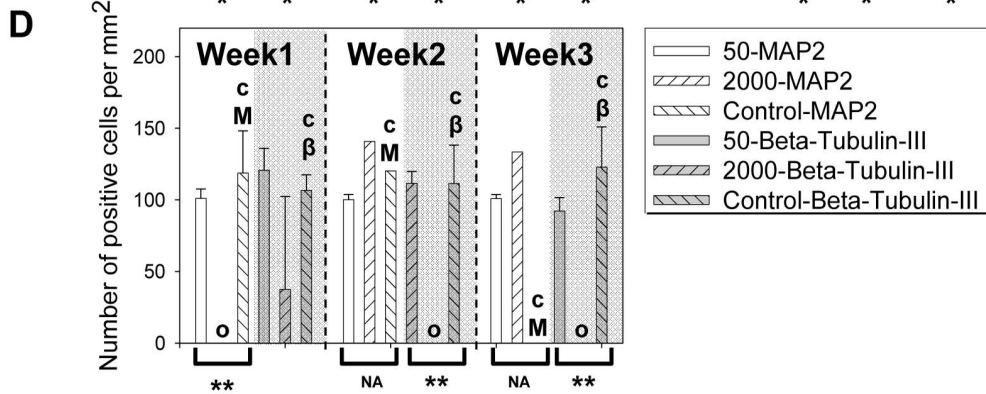
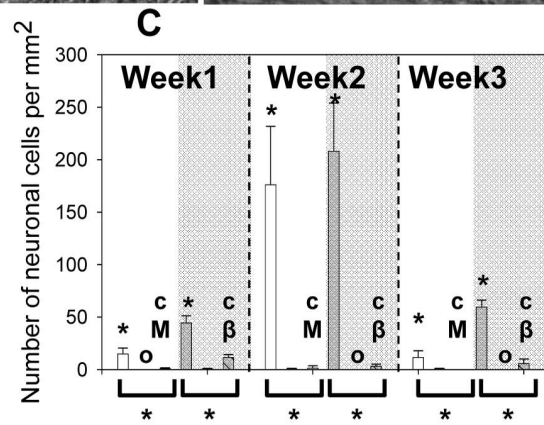
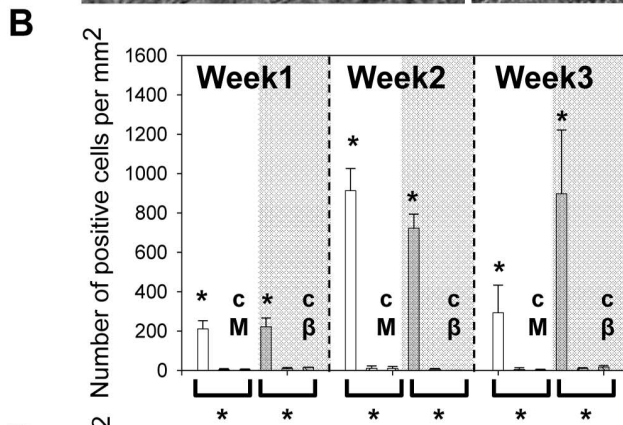
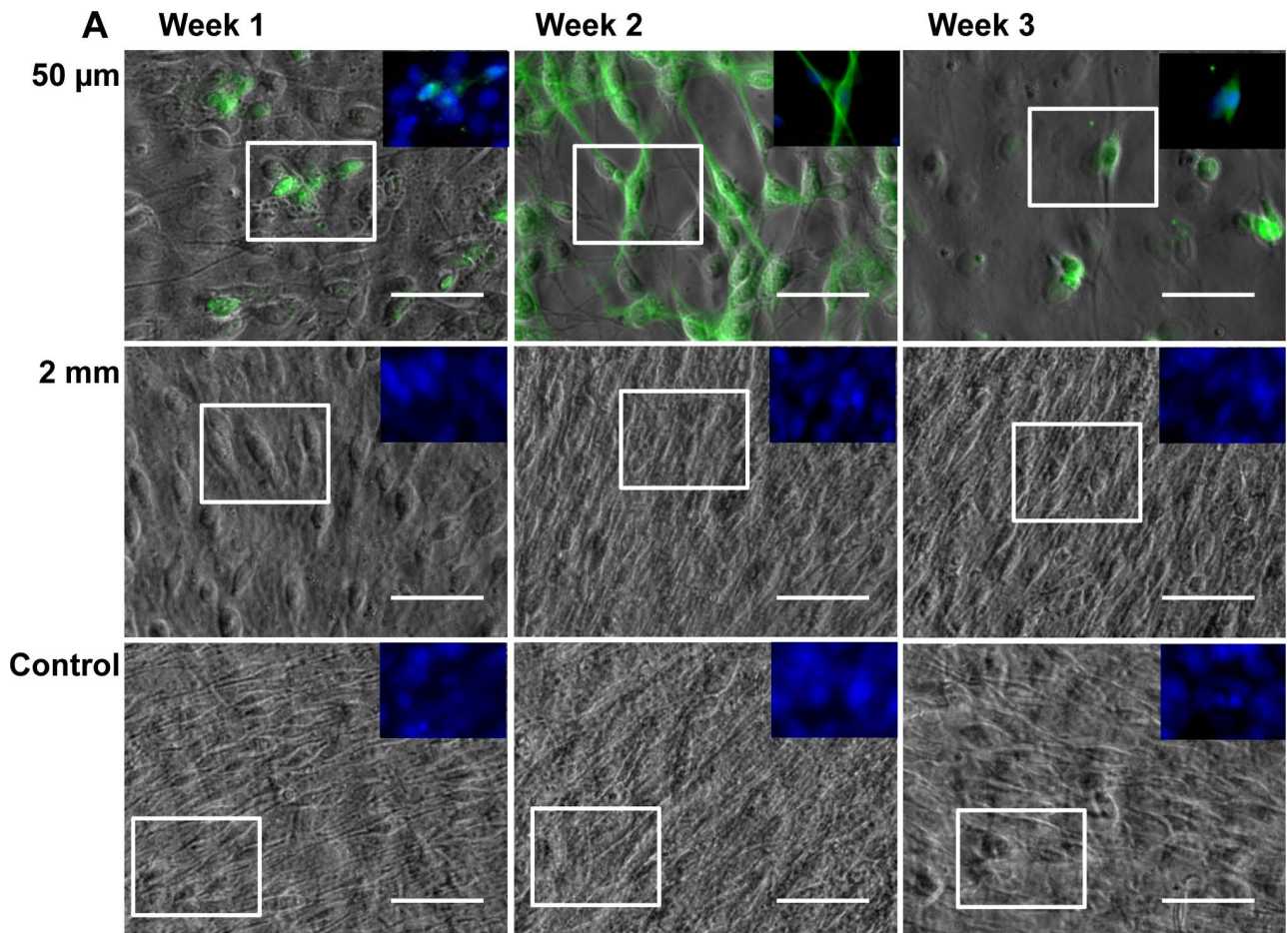


Figure 6. C17.2 cells behavior characterized by MAP2 staining. (A) The morphology of cells shown as overlaid phase contrast and MAP2 staining images. Green: MAP2. Blue: cell nuclei. Scale bar = 50 μm . The insets of MAP2 and cell nuclei staining were from the boxed region and were at the same scale as the main images. (B) MAP2 and β -tubulin-III (gray shades) positive cell counts per mm^2 over three weeks. Both staining showed similar trend of cell differentiation versus test conditions. (C) The neuronal cell count per mm^2 over time determined by cell morphology plus MAP2 or β -tubulin-III (gray shades) staining. (D) The average neurite length per mm^2 over time with positive MAP-2 or β -tubulin-III (gray shades) staining. The controls (with "cM" for MAP2 control and "c β " for β -tubulin-III control) were C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. Bars with "O" in Figure 6C and Figure 6D indicated that no cell was identified as a neuronal cell. Data were shown as mean \pm standard deviation. The * above the bars indicated a statistical difference between the sample and the control by two-tailed Student's t test ($p < 0.05$). The */** below the bars indicated a statistical difference in the group by the one-way ANOVA test ($p < 0.05$). The ** in Figure 6D indicated a significant difference due exclusively to the samples with no neurite outgrowth. The groups labeled with NA below the brackets did not have enough number of neurites for ANOVA analysis. $N \geq 15$.
doi:10.1371/journal.pone.0109815.g006

heights and long feeding intervals is a result of nutrient consumption, not PDMS or the flow feeding.

Confirmation of Differentiation by MAP2 staining

MAP2 staining was carried out in selected samples to confirm the differentiation characterization by β -tubulin-III staining. Here a MAP2 antibody targeting both MAP2a (expressed constitutively in neuronal cells) and MAP2b (expressed postnatal) isoforms was selected, so it stained differentiated neuronal cells at similar stages as the β -tubulin-III antibody. The selected culture conditions are: 1) a condition in microchannels with the highest level of differentiation, i.e. 50 μm tall microchannel samples under a 48 hr feeding interval, 2) a condition in microchannels with MF equivalent to that of the control, i.e. 2 mm tall microchannel samples under a 48 hr feeding interval and 3) the open culture control, i.e. fluorodish samples under a 48 hr feeding interval. The morphology of the cells is shown in Figure 6A with MAP2 staining (green) overlaid with the phase contrast images. The insets show the overlaid MAP2 and nuclei staining. MAP2 staining was

obvious only in the 50 μm samples, but not the other two. The expression of MAP2 peaked at week 2 and decreased at week 3.

The quantitative analysis of MAP2 staining is shown in Figure 6B-6D together with that of the β -tubulin-III staining. The 50 μm microchannel samples demonstrated higher level of differentiation than the control (Figure 6B) marked by MAP2 and β -tubulin-III expression (with * above, p range from 0.0001 to 0.007) while both biomarkers demonstrated cells in the 2000 μm microchannels to be comparable to the control (p range from 0.66 to 0.96). When neuronal cells were counted by positive MAP2 staining and neurite outgrowth greater than twice of the cell body, the dependence of neuronal cell density on the culture condition were comparable to the findings from β -tubulin-III staining (Figure 6C). MAP2 staining showed initiation, peak and degeneration of neuronal differentiation in the 50 μm microchannels similar to β -tubulin-III staining. The neurite length determined from MAP2 positive cells was found to be mostly comparable to the control at the same week, consistent with the results from β -tubulin-III staining (Figure 6D). However, the number of neurites in the MAP2 stained samples was not large enough to carry out

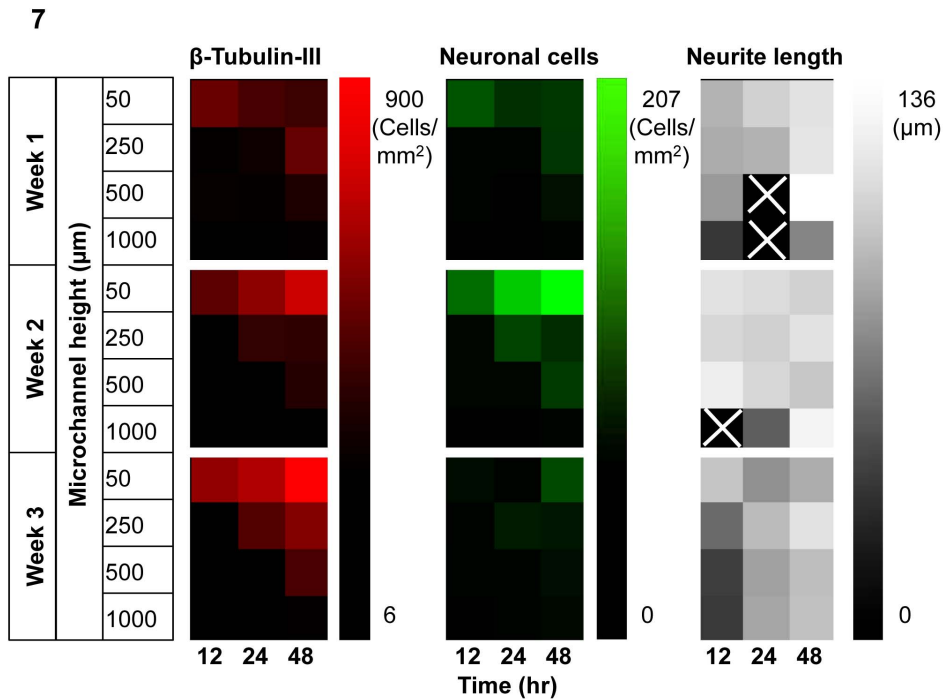


Figure 7. Summary of cell phenotypes with microchannel heights of 50 μm to 1000 μm and feeding frequencies of 12 hours to 48 hours. Groups with small MFs (towards top right corner of each graph) generally had more obvious neuronal cell differentiation as demonstrated by brighter colors representing higher density of cells with positive β -tubulin-III staining and neural morphology (first and second columns). The neurite length (third column), however, did not seem to have a strong correlation with the MF. The samples without noticeable neurite outgrowth were marked with a cross sign.
doi:10.1371/journal.pone.0109815.g007

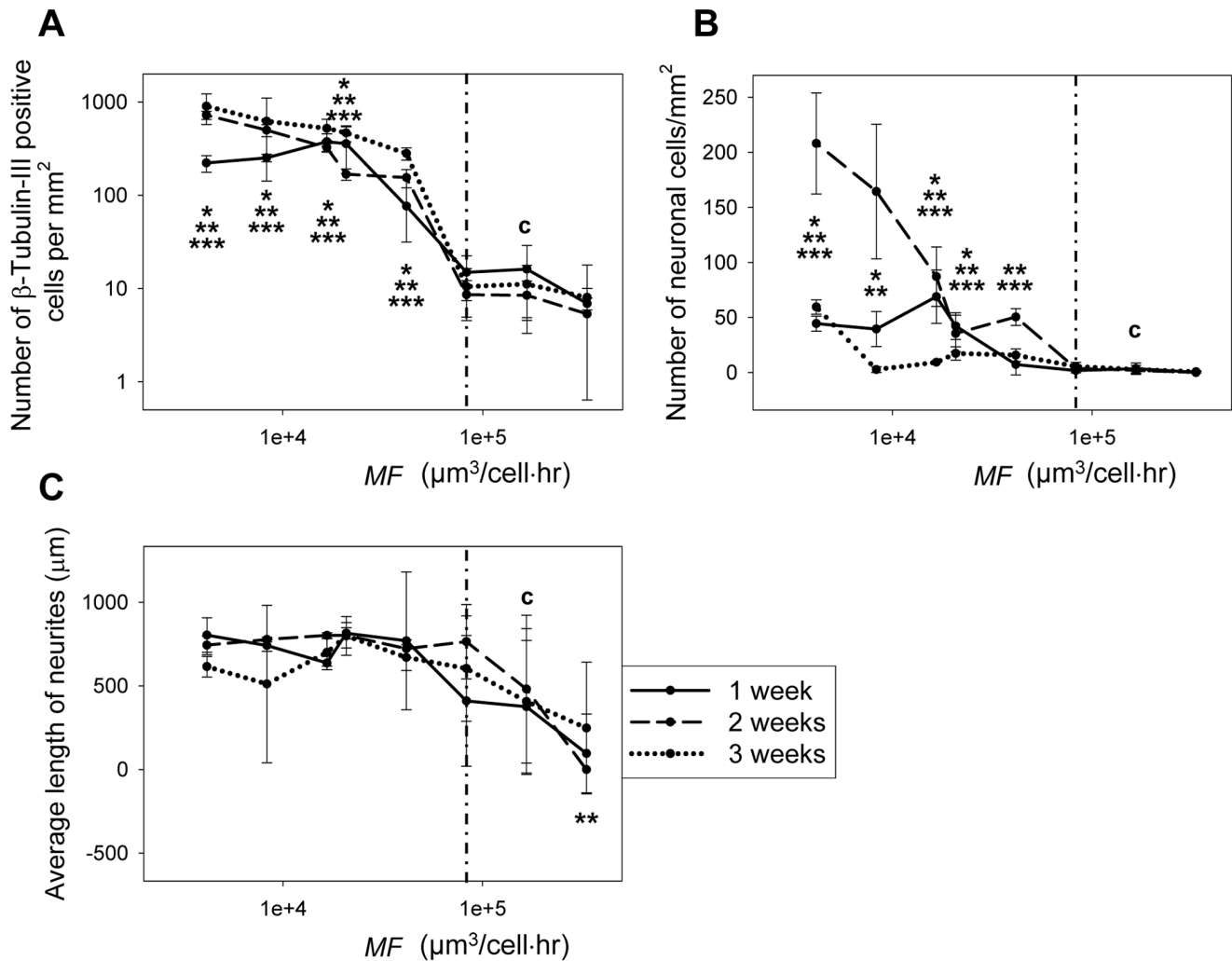


Figure 8. Correlation between MF and neuronal cell differentiation. (A) Samples with MF number smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ had significantly higher numbers of β -tubulin-III positive cells than that of the control. Samples with MF numbers equal to or larger than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ had similar β -tubulin-III positive cell population compared to the control. (B) Samples with MFs smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ generally had significantly higher numbers of neuronal cells while samples with MFs equal to or larger than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ were mostly comparable to the control. (C) The average neurite length had minimal correlation with the MF. The control (with "c") was C17.2 NSCs seeded at the same surface density in FluoroDishes but without microchannels and fed every 48 hours as in standard subculture protocols. In all data points, $N \geq 15$. * indicates statistical difference compared to the control after 1 week, ** for 2 weeks and *** for 3 weeks ($p < 0.05$). The vertical dash line represents the critical MF of $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$. doi:10.1371/journal.pone.0109815.g008

ANOVA analysis (groups labeled with NA below brackets). The comparable staining results of MAP2 and β -tubulin-III support our method of identifying differentiated neuronal cells by β -tubulin-III staining.

Correlation of the MF to neuronal cell differentiation

To quantify the average amount of medium available to cells over time, the MF was introduced, which is the amount of culture medium available to each cell (cell number from initial seeding) divided by the feeding interval.

As summarized in the heat maps in Figure 7, experiment groups with low MFs (top right corner of each graph) were often associated with more prominent neuronal cell differentiation marked by more cells with positive β -tubulin-III staining (red) and more neuronal cells (green) than groups with high MFs (lower left corner of each graph). The neurite length is mostly $\sim 100 \mu\text{m}$

except for those without observable neurite outgrowth (marked with a cross in the last panel of Figure 7).

Statistical analysis was carried out to quantitatively investigate the correlation between MF and neuronal cell differentiation. MF values of all experiment groups were calculated and data sets were re-organized based on their MF values. As shown from the relatively tight error bars in most data points in Figure 8, the parameter MF is the dictating factor that controls the behavior of C17.2 in standard culture media. The critical MF of $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ is indicated by the vertical dash line in Figure 8. The control is labeled with "c". Demonstrated in Figure 8A, samples with MF smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ had significantly larger numbers of β -tubulin-III positive cells than that of the control (p values range from 7×10^{-15} to 0.0004). Samples with MF numbers equal to or greater than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ had similar β -tubulin-III positive cell population compared to the control (p values range from 0.1 to 0.8). This correlation

held true over the entire experiment course of 3 weeks (* indicates statistical difference compared to the control after 1 week, ** for 2 weeks and *** for 3 weeks). The number of neuronal cells also correlated well with the MF (Figure 8B). Samples with MF s smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ generally had significantly higher numbers of neuronal cells (p range from 5×10^{-13} to 0.013) while samples with MF equal to or greater than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ were comparable (p values range from 0.1 to 1) to the control. Out of 24 data sets, only 2 fell out of this correlation, i.e. at $MF = 41,500 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ at week 1 ($p = 0.28$) and $MF = 8,300 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ at week 3 ($p = 0.9$). These two outliers were likely a result of time-dependent uprising and degeneration of the neuronal cell population over time. When further examining the morphological change of cells over time, an almost pure neuronal cell population of high density was observed at week two for groups with MF of $8.3 \times 10^3 \mu\text{m}^3/\text{cell}\cdot\text{hr}$ or smaller. On the other hand, the average neurite length mostly remained unchanged with the MF (Figure 8C) regardless of the level of spontaneous differentiation (Figure 2–6). Thus, the MF is a parameter that can be used to predict spontaneous neuronal cell differentiation in standard culture medium for C17.2 NSCs, while the neurite length is not strongly controlled by the MF .

While the microfluidic culture introduced a few differences from conventional culture, including the exposure to shear stress, presence of PDMS and rate of nutrient depletion, the nutrient availability seemed to be the main contributor to the observed spontaneous differentiation. In our preliminary studies (Figure S1, Figure S2 and Figure S3), we demonstrated that leachant from PDMS, if present, did not induce higher C17.2 differentiation than the control of conventional culture. In addition, the optimal shear stress to maintain C17.2 NSCs was found to be around 0.004 Pa. This shear stress is within the range normally experienced by NSCs *in vivo*. [65] NSCs in their natural physiological environment experience shear stress generated by interstitial flow, which falls into the range of 0.01 to 0.001 Pa. [65–70] Thus the flow condition used in the study is not expected to be detrimental to the NSCs. C17.2 cells cultured in the 2 mm-thick channel showed comparable or even lower spontaneous differentiation when compared to the conventional static culture (Figure 5), indicating the shear condition used here did not contribute to the enhanced differentiation in the thinner channels. Thus, the correlation of the cell phenotype with the MF demonstrates that MF is the major contributor to the observed high levels of spontaneous differentiation in thin devices or long feeding intervals.

Our observation of spontaneous neuronal cell differentiation under low MF is consistent with reports in the literature from *in vivo* studies: in response to nutrient depletion and the resulting damage in the neural network, NSCs go through neuronal cell differentiation in an effort to repair the damage. [4,15,16,53–58] Nutrient depletion by serum withdrawal is also the predominant method to induce neuronal differentiation of C17.2 NSCs *in vitro*. [59–61,64,71].

Although it is difficult to predict or determine the molecular source that contributes to the process, the observed critical MF suggests that the key molecules should have been consumed and reached a critically low concentration to induce spontaneous differentiation. For example, epidermal growth factor (EGF) may be an important player in neuronal cell differentiation: stem cell culture medium contains 10 ng/ml EGF while differentiation medium contains no EGF. [13,14,74–77] Based on the MF threshold, the consumption rate of EGF is predicted to be greater than 3.5×10^{-23} mol/s·cell. This prediction is consistent with experimental measurements that places consumption rate of EGF

at 3.4×10^{-22} mol/s·cell for a fast EGF consuming cell model A431 epidermoid carcinoma cells. [78] Thus, the MF threshold identified here may offer insight about the consumption rates of key chemicals involved in neuronal cell differentiation.

As observed in all the samples showing NSC differentiation, the neuronal cell population experienced a dynamic process of growth, peak and degeneration over the 3 week culture period. Although neurons are terminally differentiated cells and cannot proliferate, [1,79–82] primary neurons are capable of surviving *in vitro* culture for weeks. [48,49,83] The fast degeneration of the spontaneously differentiated neuronal cells in the case described herein may be caused by two possible reasons: an unfavorable environment to maintain neuronal cells and lack of an integrated neuronal cell network that is often required for long-term neuronal survival *in vitro*. The culture medium and feeding pattern was optimized for culturing NSCs instead of neuronal cells. Although neuronal cells can differentiate spontaneously from NSCs through nutrient consumption, maintaining them might require medium adjustment as neural apoptosis can be induced by a variety of stimuli such as growth factor concentration change and glucose concentration change. [84–93] Additionally, neurons are much more sensitive to shear stress than NSCs, thus cell feeding through laminar flow may damage the neuronal cells. [48,49,77,94–99] The other possible cause is immaturity of neural network. The protocols to induce NSC differentiation (C17.2 cells and others) and maintain the resulting neuronal cells usually require chemical stimuli concurrent with nutrient depletion. [4,12,59–62,64,73,75] These stimuli promote the formation of dopaminergic neurons and neural communication, which are key to their integration in certain areas of the brain. [2–5,11,12,16,81] The neuronal cells formed in this study by nutrient consumption alone may lack the proper cues to integrate into a network, thus degenerate soon after differentiation.

While the cell population and nutrient availability are widely different in this study, the neurite outgrowth length appears consistent in majority of the test conditions. It has been reported that when using the same differentiation method, the length of neurites is characteristic of the physical environment. Curley et al. have reported characteristic neurite length of differentiated C17.2 NSCs on materials of different elasticity. [100] Yang et al. have used complex environmental physical cues to control both the neurite length and orientation of differentiated C17.2 NSCs. [101] The consistency of neurite outgrowth length observed in this study is likely a result of comparable physical exposures in all microfluidic samples, while the biochemical cues from nutrient restriction don't seem to play a key in neurite development after initiating NSC differentiation.

Despite the observed degeneration of differentiated neuronal cells, the β -tubulin-III positive cell population generally maintained a steady growth in our study, even after neuronal degeneration. This was a result of an emerging cell population with flattened morphology and multiple radially extended unbranched short processes in week 3. These morphological characteristics are consistent with those of intermediate cell types between NSCs and neurons. [102,103] While β -tubulin-III is often used an early neural marker, [104–106] any neuron-restricted progenitor cell type between the NSC phase and differentiated post-mitotic neuron phase could express β -tubulin-III. [107–109] The continuous proliferation of the intermediate cells kept the β -tubulin-III positive cell on the rise, [76,102,110–114] however, they were incapable of replacing the degenerated neuronal cells in the culture environment studied here. Our observation suggests different signals and culture environments may be required for the

branched differentiation pathways from C17.2 NSCs to neuronal cells and from intermediate cells to neuronal cells.

Conclusions

The *MF* successfully predicts the outcome of C17.2 NSCs in standard culture medium. The *MF* smaller than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hour}$ causes spontaneous neuronal cell differentiation marked by a higher density of cells with positive β -tubulin-III or MAP2 staining and neural morphology than the control. On the other hand, minimal spontaneous neuronal cell differentiation is observed when the *MF* is equal to or larger than $8.3 \times 10^4 \mu\text{m}^3/\text{cell}\cdot\text{hour}$. The average neurite length does not have a strong correlation with the *MF*. The *MF* can be controlled by several experimental factors such as cell density, cell medium volume and feeding time interval to maintain the stem cell status of C17.2 NSCs or to induce various levels of neuronal cell differentiation. Thus, the findings offer guidelines to microfluidic system design for controllable NSC maintenance and differentiation.

Supporting Information

Figure S1 Cell adhesion and proliferation in 50 μm microchannel with continuous flow of regular stem cell culture medium. C17.2 cell adhesion and proliferation was tested in 50 μm tall microchannel with continuous flow of 1, 2, 3 and 4 $\mu\text{L}/\text{hour}$. (S1.A–S1.D) Cell morphologies after 1 day of continuous flow of medium at different flow rates. (S1.E) The surface area covered by cells after 1 day of culture was normalized to that after 3 hour of static adhesion (S1.E) to estimate the number of cells in the microchannels. Continuous medium feeding at 3 $\mu\text{L}/\text{hour}$ yielded the highest number of adherent cells after 1 day of continuous flow, but little cell proliferation was observed. Scale bar = 100 μm . $N \geq 15$. (TIF)

Figure S2 Cell adhesion and proliferation in 50 μm microchannel with periodic flow of regular stem cell culture medium. C17.2 cell adhesion and proliferation was tested in 50 μm tall microchannel with periodic flow of 50, 150,

250, 350, 450 and 550 $\mu\text{L}/\text{hour}$ administered every 12 hours. (S2.A–S2.D) Cell morphologies after 1 day of continuous flow of medium at different flow rates. (S2.E) The surface area covered by cells after 1 day of culture is normalized to that after 3 hour of static adhesion (S2.E) to estimate the number of cells in the microchannels. Periodic medium feeding at 250 $\mu\text{L}/\text{hour}$ every 12 hours yielded the highest number of adherent cells and significant cell proliferation after 1 day of continuous flow. Scale bar = 100 μm . $N \geq 15$.

(TIF)

Figure S3 Cell adhesion and proliferation under different frequencies. C17.2 cell adhesion and proliferation was tested under different feeding frequencies in 50 μm tall microchannel with a periodic flow of 250 $\mu\text{L}/\text{hour}$. (S3.A–S3.D) Cell morphologies after 1 day of continuous flow of regular stem cell culture medium at different flow rates. (S3.E) The surface area covered by cells after 1 day of culture was normalized to that after 3 hour of static adhesion to estimate the number of cells in the microchannels. Periodic medium feeding at 250 $\mu\text{L}/\text{hour}$ administered every 12 hours yielded the highest number of adherent cells after 1 day of continuous flow. Feeding periods less than 12 hours led to significant less adherent cells in the device. Thus, only feeding periods of 12 hours or higher were used in the work. Scale bar = 100 μm . $N \geq 15$.

(TIF)

Acknowledgments

This work was supported by the National Science Foundation (CBET-1014957). We are grateful for Evan Snyder from the Sanford-Burnham Medical Research Institute for a generous gift of C17.2 NSCs, Emily Geishecker and Meghan E. Casey from Lehigh University for immunocytochemistry protocols and helpful discussions on the project.

Author Contributions

Conceived and designed the experiments: BW SJ XC. Performed the experiments: BW. Analyzed the data: BW. Contributed reagents/materials/analysis tools: BW SJ XC. Wrote the paper: BW. Proof Reading: SJ XC.

References

- Zhao CM, Deng W, Gage FH (2008) Mechanisms and functional implications of adult neurogenesis. *Cell* 132 (4) 645–660.
- Bjorklund LM, Sanchez-Pernaute R, Chung SM, Andersson T, Chen IYC, et al. (2002) Embryonic stem cells develop into functional dopaminergic neurons after transplantation in a Parkinson rat model (2002). *Proceedings of the National Academy of Sciences of the United States of America* 99 (4) 2344–2349.
- Kim JH, Auerbach JM, Rodriguez-Gomez JA, Velasco I, Gavin D et al. (2002) Dopamine neurons derived from embryonic stem cells function in an animal model of Parkinson's disease. *Nature* 418 (6893) 50–56.
- Bjorklund A, Lindvall O (2003) Cell replacement therapies for central nervous system disorders. *Nat. Neurosci.* 6 (6) 537–544.
- Wernig M, Zhao JP, Pruszak J, Hedlund E, Fu DD, et al. (2008) Neurons derived from reprogrammed fibroblasts functionally integrate into the fetal brain and improve symptoms of rats with Parkinson's disease. *Proceedings of the National Academy of Sciences of the United States of America* 105 (15) 5856–5861.
- Nakatomi H, Kuriu T, Okabe S, Yamamoto S, Hatano O, et al. (2002) Regeneration of hippocampal pyramidal neurons after ischemic brain injury by recruitment of endogenous neural progenitors. *Cell* 110 (4) 429–441.
- Chen JL, Li Y, Wang L, Zhang ZG, Lu DY, et al. (2001) Therapeutic benefit of intravenous administration of bone marrow stromal cells after cerebral ischemia in rats. *Stroke* 32 (4) 1005–1011.
- Arvidsson A, Collin T, Kirik D, Kokaia Z, Lindvall O (2002) Neuronal replacement from endogenous precursors in the adult brain after stroke. *Nat. Med.* 8 (9) 963–970.
- Yang M, Stull ND, Berk MA, Snyder EY, Iacovitti L (2002) Neural stem cells spontaneously express dopaminergic traits after transplantation into the intact or 6-hydroxydopamine-lesioned rat. *Exp. Neurol.* 177 (1) 50–60.
- Snyder EY, Deitcher DL, Walsh C, Arnoldaldea S, Hartwig EA, et al. (1992) Multipotent Neural Cell-Lines Can Engraft and Participate in Development of Mouse Cerebellum. *Cell* 68 (1) 33–51.
- Ryu MY, Lee MA, Ahn YH, Kim KS, Yoon SH, et al. (2005) Brain transplantation of neural stem cells cotransduced with tyrosine hydroxylase and GTP cyclohydrolase 1 in parkinsonian rats. *Cell Transplant.* 14 (4) 193–202.
- Liu WG, Lu GQ, Li BA, Chen SD (2007) Dopaminergic neuroprotection by neurturin-expressing c17.2 neural stem cells in a rat model of Parkinson's disease. *Parkinsonism Relat. Disord.* 13 (2) 77–88.
- Akerud P, Canals JM, Snyder EY, Arenas E (2001) Neuroprotection through delivery of glial cell line-derived neurotrophic factor by neural stem cells in a mouse model of Parkinson's disease. *Journal of Neuroscience* 21 (20) 8108–8118.
- Pineda JR, Rubio N, Akerud P, Urban N, Badimon L, et al. (2007) Neuroprotection by GDNF-secreting stem cells in a Huntington's disease model: optical neuroimage tracking of brain-grafted cells. *Gene Ther.* 14 (2) 118–128.
- Sinden JD, RashidDoubell F, Kershaw TR, Nelson A, Chadwick A, et al. (1997) A Recovery of spatial learning by grafts of a conditionally immortalized hippocampal neuroepithelial cell line into the ischaemia-lesioned hippocampus. *Neuroscience* 81 (3) 599–608.
- Zhu JM, Zhao YY, Chen SD, Zhang WH, Lou L, et al. (2011) Functional Recovery after Transplantation of Neural Stem Cells Modified by Brain-derived Neurotrophic Factor in Rats with Cerebral Ischaemia. *J. Int. Med. Res.* 39 (2) 488–498.
- Singh A, Suri S, Lee T, Chilton JM, Cooke MT, et al. (2013) Adhesion strength-based label-free isolation of human pluripotent stem cells. *Nature Methods* 10 (5) 438–+.

18. Loewke KE, Camarillo DB, Piyawattanametha W, Mandella MJ, Contag CH, et al. (2011) In Vivo Micro-Image Mosaicing. *IEEE Trans. Biomed. Eng.* 58 (1) 159–171.
19. Solanki A, Chueng STD, Yin PT, Kappera R, Chhowalla M, et al. (2013) Axonal Alignment and Enhanced Neuronal Differentiation of Neural Stem Cells on Graphene-Nanoparticle Hybrid Structures. *Adv. Mater.* 25 (38) 5477–5482.
20. Jung DJ, Minami I, Patel S, Lee J, Jiang B, et al. (2012) Incorporation of functionalized gold nanoparticles into nanofibers for enhanced attachment and differentiation of mammalian cells. *J. Nanobiotechnol.* 10 10.
21. Cimetta E, Figallo E, Cannizzaro C, Elvassore N, Vunjak-Novakovic G (2009) Micro-bioreactor arrays for controlling cellular environments: Design principles for human embryonic stem cell applications. *Methods* 47 (2) 81–89.
22. Park JY, Kim SK, Woo DH, Lee E, Kim JH, et al. (2009) Differentiation of Neural Progenitor Cells in a Microfluidic Chip-Generated Cytokine Gradient. *Stem Cells* 27 (11) 2646–2654.
23. Park JY, Takayama S, Lee SH (2010) Regulating microenvironmental stimuli for stem cells and cancer cells using microsystems. *Integrative Biology* 2 (5–6) 229–240.
24. Yu HM, Meyvantsson I, Shkel IA, Beebe DJ (2005) Diffusion dependent cell behavior in microenvironments. *Lab Chip* 5 (10) 1089–1095.
25. Zhang H, Liu KK (2008) Optical tweezers for single cells *Journal of the Royal Society Interface* 5 (24) 671–690.
26. Cai L, Friedman N, Xie XS (2006) Stochastic protein expression in individual cells at the single molecule level. *Nature* 440 (7082) 358–362.
27. Warren L, Bryder D, Weissman IL, Quake SR (2006) Transcription factor profiling in individual hematopoietic progenitors by digital RT-PCR. *Proceedings of the National Academy of Sciences of the United States of America* 103 (47) 17807–17812.
28. Zhong JF, Chen Y, Marcus JS, Scherer A, Quake SR, et al. (2008) A microfluidic processor for gene expression profiling of single human embryonic stem cells. *Lab Chip* 8 (1) 68–74.
29. Kraus T, Verpoorte E, Linder V, Franks W, Hierlemann A, et al. (2006) Characterization of a microfluidic dispensing system for localised stimulation of cellular networks. *Lab Chip* 6 (2) 218–229.
30. Park TH, Shuler ML (2003) Integration of cell culture and microfabrication technology. *Biotechnol. Prog.* 19 (2) 243–253.
31. Rajaraman S, Choi SO, Shafer RH, Ross JD, Vukasinovic J, et al. (2007) Microfabrication technologies for a coupled three-dimensional microelectrode microfluidic array. *J. Micromech. Microeng.* 17 (1) 163–171.
32. Ellison D, Munden A, Levchenko A (2009) Computational model and microfluidic platform for the investigation of paracrine and autocrine signaling in mouse embryonic stem cells. *Mol. Biosyst.* 5 (9) 1004–1012.
33. Wan CR, Chung S, Kamm RD (2011) Differentiation of Embryonic Stem Cells into Cardiomyocytes in a Compliant Microfluidic System. *Annals of Biomedical Engineering* 39 (6) 1840–1847.
34. Hemmingsen M, Vedel S, Skafte-Pedersen P, Sabourin D, Collas P, et al. (2013) The Role of Paracrine and Autocrine Signaling in the Early Phase of Adipogenic Differentiation of Adiposederived Stem Cells. *PLoS One* 8 (5) 14.
35. Khetani SR, Bhatia SN (2006) Engineering tissues for in vitro applications. *Curr. Opin. Biotechnol.* 17 (5) 524–531.
36. Trkov S, Eng G, Di Liddo R, Parnigotto P, Vunjak-Novakovic G (2010) Micropatterned three-dimensional hydrogel system to study human endothelial-mesenchymal stem cell interactions. *J. Tissue Eng. Regen. Med.* 4 (3) 205–215.
37. Zhong WL, Tian K, Zheng XF, Li LN, Zhang WG, et al. (2013) Mesenchymal Stem Cell and Chondrocyte Fates in a Multishear Microdevice Are Regulated by Yes-Associated Protein. *Stem Cells Dev.* 22 (14) 2083–2093.
38. Labeed FH, Lu J, Mulhall HJ, Marchenko SA, Hoettges KF, et al. (2011) Biophysical Characteristics Reveal Neural Stem Cell Differentiation Potential. *PLoS One* 6 (9) e25458.
39. Huang CP, Lu J, Seon H, Lee AP, Flanagan LA, Kim, et al. (2009) Engineering microscale cellular niches for three-dimensional multicellular co-cultures. *Lab Chip* 9 (12) 1740–1748.
40. Flanagan LA, Lu J, Wang L, Marchenko SA, Jeon NL, et al. (2008) Unique dielectric properties distinguish stem cells and their differentiated progeny. *Vol. 26 p* 656–65.
41. King KR, Wang S, Jayaraman A, Yarmush L, Toner M (2008) Microfluidic flow-encoded switching for parallel control of dynamic cellular microenvironments. *Lab Chip* 8 (1) 107–116.
42. King KR, Wang SH, Irimia D, Jayaraman A, Toner M, et al. (2007) A high-throughput microfluidic real-time gene expression living cell array. *Lab Chip* 7 (1) 77–85.
43. Huang NF, Dewi RE, Okogbua J, Lee JC, JalilRufaihah A, et al. (2013) Chemotaxis of human induced pluripotent stem cell-derived endothelial cells. *Am. J. Transl. Res.* 5 (5) 510–U96.
44. Shamloo A, Manchandia M, Ferreira M, Mani M, Nguyen C, Jahn T, et al. (2013) Complex chemoattractive and chemorepellent Kit signals revealed by direct imaging of murine mast cells in microfluidic gradient chambers. *Integrative Biology* 5 (8) 1076–1085.
45. Tavana H, Mosadegh B, Zamankhan P, Grotberg JB, Takayama S (2011) Micropatterned Feeder Cells Guide Embryonic Stem Cell Fate. *Biotechnol. Bioeng.* 108 (10) 2509–2516.
46. Chung C, Pruitt BL, Heilshorn SC (2013) Spontaneous cardiomyocyte differentiation of mouse embryoid bodies regulated by hydrogel crosslink density. *Biomaterials Science* 1 (10) 1082–1090.
47. Blagovic K, Kim LLY, Voldman J (2011) Microfluidic Perfusion for Regulating Diffusible Signaling in Stem Cells. *PLoS One* 6 (8) 11.
48. Chung BG, Flanagan LA, Rhee SW, Schwartz PH, Lee AP, et al. (2005) Human neural stem cell growth and differentiation in a gradient-generating microfluidic device. *Lab Chip* 5 (4) 401–406.
49. Wang JY, Ren L, Li L, Liu WM, Zhou J, et al. (2009) Microfluidics: A new cosset for neurobiology. *Lab Chip* 9 (5) 644–652.
50. Keenan TM, Grinager JR, Procar AA, Svendsen CN (2012) In vitro localization of human neural stem cell neurogenesis by engineered FGF-2 gradients. *Integrative Biology* 4 (12) 1522–1531.
51. Lanfer B, Hermann A, Kirsch M, Freudenberg U, Reuner U, et al. (2010) Directed Growth of Adult Human White Matter Stem Cell-Derived Neurons on Aligned Fibrillar Collagen. *Tissue Eng. Part A* 16 (4) 1103–1113.
52. Chang YJ, Tsai CJ, Tseng FG, Chen T, Wang TW (2013) Micropatterned stretching system for the investigation of mechanical tension on neural stem cells behavior. *Nanomed.-Nanotechnol. Biol. Med.* 9 (3) 345–355.
53. Jin KL, Peel AL, Mao XO, Xie L, Cottrell BA, et al. (2004) Increased hippocampal neurogenesis in Alzheimer's disease. *Proceedings of the National Academy of Sciences of the United States of America* 101 (1) 343–347.
54. Liu JL, Solway K, Messing RO, Sharp FR (1998) Increased neurogenesis in the dentate gyrus after transient global ischemia in gerbils. *Journal of Neuroscience* 18 (19) 7768–7778.
55. Zhang RL, Zhang ZG, Zhang L, Chopp M (2001) Proliferation and differentiation of progenitor cells in the cortex and the subventricular zone in the adult rat after focal cerebral ischemia. *Neuroscience* 105 (1) 33–41.
56. Horie N, So K, Moriya T, Kitagawa N, Tsutsumi K, et al. (2008) Effects of oxygen concentration on the proliferation and differentiation of mouse neural stem cells in vitro. *Cellular and Molecular Neurobiology* 28 (6) 833–845.
57. Iwai M, Sato K, Omori N, Nagano I, Manabe Y, et al. (2002) Three steps of neural stem cell development in gerbil dentate gyrus after transient ischemia. *J. Cereb. Blood Flow Metab.* 22 (4) 411–419.
58. Sun JQ, Zhou WH, Sha B, Yang Y (2010) Ischemia induced neural stem cell proliferation and differentiation in neonatal rat involved vascular endothelial growth factor and transforming growth factor-beta pathways. *Brain Dev.* 32 (3) 191–200.
59. Kim SJ, Son TG, Kim K, Park HR, Mattson MP, et al. (2007) Interferon-gamma promotes differentiation of neural progenitor cells via the JNK pathway. *Neurochemical Research* 32 (8) 1399–1406.
60. Li M, Tsang KS, Choi ST, Li K, Shaw C, et al. (2011) Neuronal Differentiation of C17.2 Neural Stem Cells Induced by a Natural Flavonoid Baicalin. *ChemBioChem* 12 (3) 449–456.
61. Lu W, Wang J, Wen TQ (2008) Downregulation of Rho-GDI gamma promotes differentiation of neural stem cells. *Molecular and Cellular Biochemistry* 311 (1–2) 233–240.
62. Bechara S, Wadman L, Popat C (2011) Electroconductive polymeric nanowire templates facilitates in vitro C17.2 neural stem cell line adhesion proliferation and differentiation. *Acta Biomater.* 7 (7) 2892–2901.
63. Lundqvist J, El Andaloussi-Lilja J, Svensson C, Dorff HG, Forsby A (2013) Optimisation of culture conditions for differentiation of C17.2 neural stem cells to be used for in vitro toxicity tests. *Toxicol. Vitro* 27 (5) 1565–1569.
64. Oh JE, Bae GU, Yang YJ, Yi, Lee HJ, et al. (2009) Cdo promotes neuronal differentiation via activation of the p38 mitogen-activated protein kinase pathway. *Faseb Journal* 23 (7) 2088–2099.
65. Qazi H, Shi ZD, Tarbell JM (2011) Fluid Shear Stress Regulates the Invasive Potential of Glioma Cells via Modulation of Migratory Activity and Matrix Metalloproteinase Expression. *PLoS One* 6 (5) 13.
66. Kurbel S (2005) Ageing and maintenance of the interstitial fluid traffic: possible roles of initial lymphatics and circadian hormones. *Med. Hypotheses* 64 (2) 375–379.
67. Deguchi Y, Inabe K, Tomiyasu K, Nozawa K, Yamada S, et al. (1995) Study on brain interstitial fluid distribution and blood-brain barrier transport of baclofen in rats by microdialysis. *Pharm. Res.* 12 (12) 1838–1844.
68. Bassar PJ (1992) Interstitial Pressure Volume and Flow During Infusion into Brain-Tissue. *Microvasc. Res.* 44 (2) 143–165.
69. Abbott NJ (2004) Evidence for bulk flow of brain interstitial fluid: significance for physiology and pathology. *Neurochem. Int.* 45 (4) 545–552.
70. Geer CP, Grossman SA (1997) Interstitial fluid flow along white matter tracts: A potentially important mechanism for the dissemination of primary brain tumors. *J. Neuro-Oncol.* 32 (3) 193–201.
71. Sharma R, Ottenhof T, Rzczkowska PA, Niles LP (2008) Epigenetic targets for melatonin: induction of histone H3 hyperacetylation and gene expression in C17.2 neural stem cells. *Journal of Pineal Research* 45 (3) 277–284.
72. Wang HF, Cheng H, Wang K, Wen TQ (2012) Different effects of histone deacetylase inhibitors nicotinamide and trichostatin A (TSA) in C17.2 neural stem cells. *J. Neural Transm.* 119 (11) 1307–1315.
73. Yang Y, Ren WW, Chen FX (2006) Knockdown of Stat3 in C17.2 neural stem cells facilitates the generation of neurons: a possibility of transplantation with a low level of oncogene. *Neuroreport* 17 (3) 235–238.
74. Kitchens DL, Snyder EY, Gottlieb DI (1994) FGF and EGF are mitogens for immortalized neural progenitors. *J. Neurobiol.* 25 (7) 797–807.

75. Garcez RC, Teixeira BL, Schmitt SD, Alvarez-Silva M, Trentin AG (2009) Epidermal Growth Factor (EGF) Promotes the In Vitro Differentiation of Neural Crest Cells to Neurons and Melanocytes. *Cellular and Molecular Neurobiology* 29 (3) 1087–1091.
76. Schwindt TT, Motta L, Barnabe F, Massant CG, Guimaraes AO, et al. (2009) Effects of FGF-2 and EGF removal on the differentiation of mouse neural precursor cells. *An. Acad. Bras. Cienc.* 81 (3) 443–452.
77. Trinh NTN, Prive A, Kheir L, Bourret JC, Hijazi T, et al. (2007) Involvement of K-ATP and KvLQT1 K⁺ channels in EGF-stimulated alveolar epithelial cell repair processes. *Am. J. Physiol.-Lung Cell. Mol. Physiol.* 293 (4) L870–L882.
78. Masui H, Castro L, Mendelsohn J (1993) Consumption of EGF by A431 cells - evidence for receptor recycling. *Journal of Cell Biology* 120 (1) 85–93.
79. Schmetsdorf S, Gartner U, Arendt T (2005) Expression of cell cycle-related proteins in developing and adult mouse hippocampus. *Int. J. Dev. Neurosci.* 23 (1) 101–112.
80. Yang Y, Herrup K (2007) Cell division in the CNS: Protective response or lethal event in post-mitotic neurons? *Biochim. Biophys. Acta-Mol. Basis Dis.* 1772 (4) 457–466.
81. Abrous DN, Koehl M, Le Moal M (2005) Adult neurogenesis: From precursors to network and physiology. *Physiol. Rev.* 85 (2) 523–569.
82. Alvarez-Buylla A, Garcia-Verdugo JM, Tramontin AD (2001) A unified hypothesis on the lineage of neural stem cells. *Nature Reviews Neuroscience* 2 (4) 287–293.
83. Millet LJ, Stewart ME, Sweedler JV, Nuzzo RG, Gillette MU (2007) Microfluidic devices for culturing primary mammalian neurons at low densities. *Lab Chip* 7 (8) 987–994.
84. Deckwerth L, Johnson EM (1993) Temporal analysis of events associated with programmed cell-death (apoptosis) of sympathetic neurons deprived of nerve growth-factor. *Journal of Cell Biology* 123 (5) 1207–1222.
85. Dimagl U, Iadecola C, Moskowitz MA (1999) Pathobiology of ischaemic stroke: an integrated view *Trends Neurosci.* 22 (9) 391–397.
86. Dugan LL, Turetsky DM, Du C, Lobner D, Wheeler M, et al. (1997) Carboxyfullerenes as neuroprotective agents. *Proceedings of the National Academy of Sciences of the United States of America* 94 (17) 9434–9439.
87. Liu XZ, Xu XM, Hu R, Du C, Zhang SX, et al. (1997) Neuronal and glial apoptosis after traumatic spinal cord injury. *Journal of Neuroscience* 17 (14) 5395–5406.
88. Yu ZF, Luo H, Fu WM, Mattson MP (1999) The endoplasmic reticulum stress-responsive protein GRP78 protects neurons against excitotoxicity and apoptosis: Suppression of oxidative stress and stabilization of calcium homeostasis. *Exp. Neurol.* 155 (2) 302–314.
89. Loo DT, Copani A, Pike CJ, Whittemore ER, Walencewicz AJ, Cotman CW (1993) Apoptosis is induced by beta-amyloid in cultured central-nervous-system neurons. *Proceedings of the National Academy of Sciences of the United States of America* 90 (17) 7951–7955.
90. Raff MC, Barres BA, Burne JF, Coles HS, Ishizaki Y, et al. (1993) Programmed cell-death and the control of cell-survival - lessons from the nervous-system. *Science* 262 (5134) 695–700.
91. Xia ZG, Dickens M, Raingeaud J, Davis RJ, Greenberg ME (1995) Opposing Effects of Erk and Jnk-P38 Map Kinases on Apoptosis. *Science* 270 (5240) 1326–1331.
92. Yao RJ, Cooper GM (1995) Requirement for phosphatidylinositol-3 kinase in the prevention of apoptosis by nerve growth-factor. *Science* 267 (5206) 2003–2006.
93. Yuan JY, Yankner BA (2000) Apoptosis in the nervous system. *Nature* 407 (6805) 802–809.
94. Colleen T Curley KF and Sabrina S Jedlicka (2012) Characterizing the effect of substrate stiffness on neural stem cell differentiation. *Mater. Res. Soc. Symp. Proc.* 1498.
95. Yang F, Murugan R, Wang S, Ramakrishna S Electrospinning of nano/micro scale poly(L-lactic acid) aligned fibers and their potential in neural tissue engineering. *Biomaterials* 26 (15) 2603–2610.
96. King JA, Miller WM (2005) Bioreactor development for stem cell expansion and controlled differentiation. *Curr. Opin. Chem. Biol.* (2007) 11 (4) 394–398.
97. Fan YW, Cui FZ, Hou SP, Xu QY, Chen LN, et al. (2002) Culture of neural cells on silicon wafers with nano-scale surface topograph. *Journal of Neuroscience Methods* 120 (1) 17–23.
98. Henley J, Poo M (2004) Guiding neuronal growth cones using Ca²⁺ signals. *Trends Cell Biol.* 14 (6) 320–330.
99. Tang FJ, Kalil K (2005) Netrin-1 induces axon branching in developing cortical neurons by frequency-dependent calcium signaling pathways. *Journal of Neuroscience* 25 (28) 6702–6715.
100. Pearce TM, Wilson JA, Oakes SG, Chiu SY, Williams JC (2005) Integrated microelectrode array and microfluidics for temperature clamp of sensory neurons in culture. *Lab Chip* 5 (1) 97–100.
101. Cullen DK, Vukasovic J, Glezer A, LaPlaca MC (2007) Microfluidic engineered high cell density three-dimensional neural cultures. *Journal of Neural Engineering* 4 (2) 159–172.
102. Culican SM, Baumrind NL, Yamamoto M, Pearlman AL (1990) Cortical Radial Glia - Identification in Tissue-Culture and Evidence for their Transformation to Astrocytes. *Journal of Neuroscience* 10 (2) 684–692.
103. Gierdalski M, Juliano SL (2003) Factors affecting the morphology of radial glia. *Cerebral Cortex* 13 (6) 572–579.
104. Fanarraga ML, Avila J, Zabala JC (1999) Expression of unphosphorylated class III beta-tubulin isotype in neuroepithelial cells demonstrates neuroblast commitment and differentiation. *Eur. J. Neurosci.* 11 (2) 517–527.
105. Katsetos CD, Nakahara C, Agamanolis DP, Karkavelas G, Lebenthal E, et al. (1994) Localization of the Neuronal Class-III Beta-Tubulin Isotype in Foci of Early Neurogenesis Supports Divergent Neuroblastic Differentiation Potential in Wilms-Tumors. *Arch. Pathol. Lab. Med.* 118 (10) 1002–1006.
106. Roskams AJ, Cai X, Ronnett GV (1998) Expression of neuron-specific beta-III tubulin during olfactory neurogenesis in the embryonic and adult rat. *Neuroscience* 83 (1) 191–200.
107. Bain G, Kitchens D, Yao M, Huettner JE, Gottlieb DI (1995) Embryonic Stem-Cells Express Neuronal Properties In-Vitro. *Developmental Biology* 168 (2) 342–357.
108. Ginis I, Luo, Miura T, Thies S, Brandenberger R, et al. (2004) Differences between human and mouse embryonic stem cells. *Developmental Biology* 269 (2) 360–380.
109. Roy NS, Wang S, Jiang L, Kang J, Benraiss A, et al. (2000) In vitro neurogenesis by progenitor cells isolated from the adult human hippocampus. *Nat. Med.* 6 (3) 271–277.
110. Anton ES, Marchionni MA, Lee KF, Rakic P (1997) Role of GGF/neuregulin signaling in interactions between migrating neurons and radial glia in the developing cerebral cortex. *Development* 124 (18) 3501–3510.
111. Diers-Fenger M, Kirchoff F, Kettenmann H, Levine JM, Trotter J (2001) AN2/NG2 protein-expressing glial progenitor cells in the murine CNS: Isolation differentiation and association with radial glia. *Glia* 34 (3) 213–228.
112. Bultje RS, Castaneda-Castellanos DR, Jan LY, Jan YN, Kriegstein AR, et al. (2009) Mammalian Par3 Regulates Progenitor Cell Asymmetric Division via Notch Signaling in the Developing Neocortex. *Neuron* 63 (2) 189–202.
113. Sevc J, Daxnerova Z, Miklosova M (2009) Role of Radial Glia in Transformation of the Primitive Lumen to the Central Canal in the Developing Rat Spinal Cord. *Cellular and Molecular Neurobiology* 29 (6–7) 927–936.
114. Zhang Y, Niu BH, Yu DM, Cheng XS, Liu B, et al. (2010) Radial glial cells and the lamination of the cerebellar cortex. *Brain Structure & Function* 215 (2) 115–122.