Supporting Information for
Prediction of antibacterial activity from physicochemical properties of antimicrobial peptides

1 Analysis of published data

Published data regarding thresholds in the membrane is not always clearly presented as the bound P:L ratio. Instead, the global P:L ratio is often found. This ratio is not as accurate as the local ratio as no information is provided on the amount of peptide that is actually bound to the membrane. If Kp and the sample volume are known, a global ratio can be corrected, but if no binding information is available approximations must be made: a shortcut to obtaining the local ratio without exact knowledge of Kp is to consider Kp very close to 1, in which case the global P:L ratio will tend to the value of the local ratio. From Eq. (2) in the main article it can be seen that this is valid if [L] is large enough so that KpγL[L] is much greater than 1. For a Kp of 5 × 104 more than 90% of bound peptide will be attained for [L] greater than 0.3 mM. Because many studies with AMPs are in such conditions, one can usually approximate the global P:L ratio as the local one, if no better alternatives are available.

2 Influence of the anionic charge of the membrane models

As stated in the main text, the use of a 2:1 POPG:POPC membrane system, instead of a system with roughly half the anionic charge density, may depart from physiological relevance. It is therefore important to assess how the increased anionicity may impact the conclusions in this work.

The MIC prediction will essentially depend on how the the Kp and threshold ratio are affected by an increased membrane anionic charge. From data on BP100 [1] it can be seen that although the Kp value increases with the anionic content of the membrane it remains in the 10^4 order of magnitude. On the other hand, thresholds involving charge events (such as full or partial charge neutralization) can be expected to vary proportionally to the increase in anionic content—corresponding in this case to a twofold increase. These variations in Kp and P:L can be approximated by using the full Kp definition [2]:

$$K_p = \frac{n_{p,L}}{n_{p,W}} \approx 1 + \frac{[P]_L}{[P]_W}$$

$$\Leftrightarrow [P]_L = \frac{K_p[P]_W}{1 - \gamma_L K_p[P]_W}$$

where γL and γW are, respectively, the molar volumes of the lipid and water molecules; the approximation in the expression can be made after assuming n_{p,W} ≪ nW. Using Eqs. (1) (of the main article) and (1), the relative change in the [P]L value upon correction can be obtained (the 'c' subscript denotes a corrected parameter):

$$[P]_{L,c} = \frac{K_{p,c} \cdot [P]_{W,c}}{K_p \cdot [P]_W}$$

One can assume that Kp values, being calculated away from excessively high peptide densities in the membrane, are equivalent to K_{p,c}. In addition, admitting that [P]_W will not change significantly in vivo (see main text), [P]_{W,c} can be made approximately equal to [P]_W. Thus,

$$\frac{[P]_{L,c}}{[P]_L} = \frac{1}{1 - \gamma_L K_{p,c} [P]_W} = \frac{1}{1 - \gamma_L K_p [P]_W} = 1 - P:L$$

This correction, even at [P]L = 130mM (P:L = 1:10), amounts to a difference of only 11% in the corrected concentration. Furthermore, it is a correction in the direction of higher bound concentrations. Rather than invalidating any of the conclusions in the analysis this further approximates the results to saturation.
It should be borne in mind that, besides the above correction, the entire partition formalism as presented here is based on the assumption of the two phases being ideally diluted solutions (i.e. the peptide molecules are dilute enough not to significantly interact with each other). As one approaches high extents of membrane coverage this assumption is inevitably invalidated. However, the fact that peptide vs. lipid fluorescence curves for BP100 and omiganan are essentially linear up to membrane saturation [1, 3] suggests that there is little error introduced by having high bound concentrations, in that range of conditions. This means that the partition equilibrium approach is valid to calculate bound concentrations at threshold points that occur below, or at, the membrane saturation point.

4 Conversion from other constants

A different binding constant, $K_b$ ($M^{-1}$)–or its inverse, the dissociation constant $K_d$ ($M$)–is also commonly used, where it is assumed that the peptide interacts with the membrane phospholipids to form a 1:1 complex [4] with reaction equilibrium constant $K_b$; the validity of this approach to interpret membrane partitioning is discussed elsewhere [2, 5]. Because published data are sometimes analyzed in this alternative framework, a conversion between both $K_p$ and $K_b$ is presented. $K_b$ is defined as:

$$K_b = \frac{[PL\text{complex}]}{[P]_{\text{free}}[L]_{\text{free}}} \approx \frac{X_L[P]}{(1 - X_L)[P][L]} = \frac{X_L}{(1 - X_L)[L]}$$

(4)

where $[PL\text{complex}]$ is the concentration of the 1:1 peptide:lipid complex, $[P]_{\text{free}}, [P], [L]_{\text{free}}$ and $[L]$ are the unbound and the total concentrations of peptide and phospholipid, respectively, and $X_L$ is the mole fraction of the bound peptide. The approximation of $[L]_{\text{free}}$ to $[L]$ significantly simplifies the calculations, but, in the case of high extents of binding, an error will be introduced. Because this approximation is roughly equivalent to the assumption of $n_{p, L} \ll n_L$ in the previous section, the resulting correction of the bound concentrations will be subject to an error of similar magnitude. Eq. (4) can be solved for $X_L$:

$$X_L = \frac{K_b[L]}{1 + K_b[L]}$$

(5)

It then becomes obvious, by comparison with Eq. (2) in the main article, that in the limit of weak interactions:

$$K_p = K_b / \gamma_L$$

(6)

References


